

# Interaction of Lipase with Lipid Model Systems

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**Abstract:** The aim of this work was to study the interaction of lipases (as an important biopolymer) with models of biomembranes based on the phospholipid and cholesterol. Lipases (triacylglycerolacyl hydrolases) are widely distributed enzymes and well-known by their hydrolytic activity. The study of the lipase interactions with lipid vesicles in aqueous dispersions is of fundamental and practical interest. The pure phosphatidylcholine from egg yolk (ePC) and cholesterol (Chol) were obtained from Sigma-Aldrich. Lipase was obtained from hog pancreas. Measurements of the current and equilibrium surface tension (ST and eST) values were carried out using a BPA-1P device and ADSA program. The particle sizes in the prepared colloidal solutions were determined by the method of dynamic light scattering. An addition of lipase led to some decrease both, of ST and eST for the samples of ePC:Chol (in the ratios from 19:1 to 1:1). The mean particle diameter (MPD) and effective particle diameter (EPD) values for the samples of ePC:Chol changed drastically by lipase addition. The EPD/MPD ratios increased from 1.7 to 2.0, from 1.8 to 2.6, from 2.3 to 6.5, from 1.5 to 2.9 for the samples of ePC:Chol at the ratios of 19:1, 14:1, 9:1, 7:1, respectively by lipase concentration increase. This general tendency can be explained by strong interaction of lipase with lipid membrane that leads to the formation of the mixed particles ePC:Chol:lipase with more narrow particle size distribution as compared to the initial EPD/MPD ratio (for the ePC:Chol mixture without lipase).

**Keywords:** Lipase, lipids, surface tension, particle size distribution.

## INTRODUCTION

In recent years, the study of the properties and applications of various lipase preparations is of high interest [1]. Lipases (triacylglycerolacyl hydrolases EC 3.1.1.3) are widely distributed enzymes [2-6] and well-known by their hydrolytic activity - the hydrolysis of fats and oils in the aqueous media [7-12]. There are numerous papers [1-12] on purification, structure-function relations and immobilization of various lipases, but the dimensions and size distributions of the lipase-containing systems are rarely described. It is important to highlight that lipase preparations are widely used in biotechnology and biomedicine, especially for therapy of the pancreas, liver and gallbladder diseases [6-13]. Recently a comparative structural and functional study of various lipases [14-16] and particular coordination between nanostructured materials and lipases for numerous applications [16-18] have been fulfilled.

The study of the effect of lipase interaction with lipid vesicles in aqueous dispersions is of fundamental and practical interest and will be a subject to discuss here.

In addition to the surface properties and enzyme activity of lipases [13], it is important to study the structural features of the lipase interaction with lipid dispersions. Such dispersions from phosphatidylcholine and other "structural lipids" which are compatible with lipid bilayer (obtained by ultrasonication or by extrusion) can be considered as the model of biological membranes (biomembranes) [19]. Biomembranes are ultra-thin, highly organized systems of molecular sizes located on the surface of cells and subcellular particles [20-22]. A necessary condition for the vital processes of a cell is a combination of such properties of biological membranes as stability and lability, the ability to self-association and molecular recognition, which is ensured by their specific chemical composition [20-22]. These properties of biomembranes are mainly due to various interactions in the lipid-protein complexes, that is why lipase addition to such lipid dispersions is very important for modeling of biomembranes [20-22]. The major lipid systems (dispersions) are well-known as liposomes, which are modeling the structure and function properties of biomembranes [23, 24].

The thickness of most biomembranes ranges from 5 to 10 nm [20-22]. Conventionally, the biomembranes are consisting of the bilayer of various types of lipids (with thickness about 3.5-5.0 nm) and proteins (integral or bound to the bilayer by non-covalent bonds). The

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lipid dispersions (sometimes called liposomes) can be roughly divided onto following systems: small unilamellar vesicle (SUVs); large unilamellar vesicle or giant unilamellar vesicles (LUVs or GUVs); multilamellar vesicle (MLVs) [20-22]. The SUV's average diameter is about 50-100 nm; MLV's – varied from 100 to 500 nm, whereas LUV's or GUV's - reaching up to 1  $\mu\text{m}$  or 100  $\mu\text{m}$  (in some special cases) [20-22]. Of course, the particular numbers are depending on the methods of measurements, for example, the MLV's average diameters varied from 100-300 nm (by electron microscopy measurements) to 150-500 nm (by light scattering measurements) for the same phospholipid's mixtures [21, 23, 24]. In this study, the authors used photon correlation spectroscopy in order to measure so-called hydrodynamic diameter ("the particle diameter plus the double layer thickness" [25]).

The most valuable phospholipids can be obtained not only from the plasma membranes, but also - from other sources, such as egg yolk [26-28]. There are egg yolk phosphatidylcholines, phosphatidylethanolamine, phosphatidylserines and others [19]. The phosphatidylcholine (PC) is one of the most important membrane phospholipids, because PC content is about half of them and PC plays the key role in the structure stability of biological membranes [28-30]. Another important natural membrane lipid is cholesterol [19, 31-34]. Cholesterol and its derivatives play the numerous roles in the membranes and total homeostasis as well as in the metabolism in cells, brain, peripheral tissues, etc. [31-33]. It is well-known that cholesterol is essential for the regulation of the biomembrane "fluidity or rigidity" [20-22], as well as for activation of mast cell and associated with obesity and diabetes in humans and animals [19, 33-35]. Cholesterol is participating in the "durability of the vesicle" that depends on its relative content in the phospholipid layer of such membrane [20-22].

Some recent studies on the structural features of the lipid monolayers as models of the biological membranes [15-17] are especially interesting for our work because they deal with the interactions of lipase with such monolayers. For example, the mentioned study presented an interesting data concerning the interactions "of recombinant dog gastric lipase (rDGL) with model monolayers liquid-liquid phase coexistence and mimicking the outer leaflet of the milk fat globule membrane" [36]. The rDGL adsorption is mainly due to combination of the hydrophobic and electrostatic interactions and "strongly impacts on the lipid phase

lateral organization" [36] that is revealed by combining some classical and modern biophysical tools such as ellipsometry, tensiometry and atomic force microscopy [36-38].

The aim of this work was to study the interaction of lipases with models of biological membranes (based on the phospholipid and cholesterol) by surface-active and light scattering measurements.

## MATERIALS AND METHODS

### Materials

The following compounds and reagents were used in this work: pure phosphatidylcholine from egg yolk (ePC) and synthetic cholesterol (Chol). These compounds were obtained from Sigma-Aldrich (Russian Federation): L- $\alpha$ -Phosphatidylcholine (Sigma-Aldrich P3556 egg yolk, Type XVI-E, lyophilized powder,  $\geq 99\%$  by TLC, CAS Number 8002-43-5); Cholesterol (Sigma-Aldrich C8667, Sigma Grade,  $\geq 99\%$  CAS Number 57-88-5).

Measurements of the current surface tension (ST) values were carried out using a BPA-1P device by the method of the maximum pressure measurements in a bubble (with a surface lifetime of 0.5 s to 10 s) [39-41].

The general principle of the device operation (based on the maximum pressure in the bubble method [39-41]) is described below [39]. The air from the compressor enters the capillary, which is lowered into the test liquid. The maximal pressure in the system is determined (Figure 1) and used to calculate the surface tension.



**Figure 1:** The tensiometer BPA-1P (adapted from [www.sinterface.de](http://www.sinterface.de) and publication [39, 41]).

This method of the maximal pressure measurement “in the buoyant bubble” allowed us to obtain the dependences of DST values vs. time (i.e., in the form of “tensiograms” [41]). All measurements were carried out at 20°C.

The equilibrium surface tension (eST) values were obtained by a calculation from the “ST vs. time” isotherms using the ADSA program [39-41]. The particle sizes in the obtained colloidal solutions were determined by the method of dynamic light scattering with the use of “90Plus/BI-MAS Particle Size Analyzer” device (Brookhaven Instruments Corporation, USA) [25]. Porcine pancreatic lipase (Lip) was obtained by purification from hog pancreas by well-known methods [1]. The data obtained were subjected to the statistical treatment by STATISTICA 10 (the average errors were below 1%).

## RESULTS

It is important to study the interaction of lipases with the lipid dispersions based on natural phospholipids: phosphatidylcholine (from egg yolk) and cholesterol. The current and equilibrium surface tension (ST and eST) values, as well as the mean particle diameter (MPD) and effective particle diameter (EPD) values for the samples of ePC:Chol from 19:1 to 1:1 (i.e. two-component mixtures of phosphatidylcholine and

cholesterol) were investigated in the presence of lipase at various concentrations.

### Lipid Dispersion ePC:Chol=19:1 in the Presence of Lipase

A lipase addition (at concentrations of 0.01, 0.05, 0.1, 0.5 and 1.0 a.u.) to the lipid dispersion (two-component mixture of ePC:Chol=19:1) led to the continuous ST decrease (Table 1) as compared to the initial mixture (72.87 mN/m at 0.5 s, 72.74 mN/m at  $t \rightarrow \infty$ ). The total decrease was from 0.85, to 1.59 mN/m by lipase addition (at maximal concentration of 1.0 a.u.) after 0.5 s and  $t \rightarrow \infty$  as compared to the initial mixture, respectively (Table 1, columns 1-5). These small changes became more pronounced (at 2.6, 4.8, 4.8, 5.0, 5.7 times) by recalculating the changes between 0.5 s and  $t \rightarrow \infty$  for each of the lipase addition (at concentrations of 0.01, 0.05, 0.1, 0.5 and 1.0 a.u., Table 1, lines 2-6, respectively), as compared to the very small changes of 0.13 mN/m for the initial mixture (72.87 mN/m at 0.5 s, 72.74 mN/m at  $t \rightarrow \infty$ ).

In general, the mean particle diameter (MPD) values decreased drastically by 11.1%, 15.8%, 23.4%, 28.5% and 41.0% by lipase addition from 0.01 to 1.0 a.u., respectively (Table 2). The effective particle diameter (EPD) values decreased almost in the same manner by 9.6%, 17.1%, 23.8%, 29.2% and 30.3% by

**Table 1: The Current and Equilibrium Surface Tension (ST and eST) Values for the Samples of ePC:Chol=19:1 as Lipid Dispersion (LD19:1) and Lipase**

Samples	t=0.5 s	t=1 s	t=3 s	t=5 s	$t \rightarrow \infty$
LD19:1 + 0.01 Lip	73.01	72.49	72.39	72.33	72.67
LD19:1 + 0.05 Lip	72.92	72.64	72.52	72.44	72.30
LD19:1 + 0.1 Lip	72.69	72.64	72.39	72.33	72.07
LD19:1 + 0.5 Lip	72.68	72.61	72.38	72.28	72.03
LD19:1 + 1.0 Lip	72.02	71.99	71.77	71.65	71.27

**Table 2: The Mean Particle Diameter (MPD) and Effective Particle Diameter (EPD) Values for the Samples of ePC:Chol=19:1 in the Presence of Lipase (Lip)**

Samples	MPD, nm	EPD, nm	EPD/MPD
LD19:1 + 0.01 Lip	202.6	350.9	1.73
LD19:1 + 0.05 Lip	191.9	321.9	1.68
LD19:1 + 0.1 Lip	174.6	296.0	1.70
LD19:1 + 0.5 Lip	162.8	275.0	1.69
LD19:1 + 1.0 Lip	134.3	270.6	2.01

lipase addition from 0.01 to 1.0 a.u., respectively (Table 2). The initial EPD and MPD values of the lipid mixture without lipase were about 388.2 and 227.8 nm, respectively.

### Lipid Dispersion ePC:Chol=14:1 in the Presence of Lipase

The total decrease was about 0.62, 0.69, 0.59, 0.56 and 0.58 mN/m by lipase addition (at maximal concentration of 1.0 a.u.) after 0.5 s, 1 s, 3 s, 5 s and  $t \rightarrow \infty$  for the mixture of ePC:Chol=14:1 as compared to the initial mixture, respectively (Table 3, columns 1-5). These small changes became more pronounced (at 5.2, 3.9, 9.8, 4.7, 4.9 times) by recalculating the changes between 0.5 s and  $t \rightarrow \infty$  for each of the lipase addition (at concentrations of 0.01, 0.05, 0.1, 0.5 and 1.0 a.u., Table 3, lines 1-5, respectively), as compared to the very small changes of 0.13 mN/m for the initial mixture (ePC:Chol=14:1).

In general, the mean particle diameter (MPD) values decreased drastically by 30.8%, 26.8%, 38.9% and 34.8% by lipase addition from 0.05 to 1.0 a.u., respectively (Table 4). The effective particle diameter (EPD) values decreased almost in the same manner by 1.4%, 2.5%, 3.8% and 9.1% by lipase addition from 0.05 to 1.0 a.u., respectively (Table 4).

### Lipid Dispersion ePC:Chol=9:1 in the Presence of Lipase

In contrast to previous data (Tables 1 and 3) the only small changes of ST values by lipase addition (at maximal concentration of 1.0 a.u.) after 0.5 s, 1 s, 3 s, 5 s and  $t \rightarrow \infty$  found for the mixture of ePC:Chol=9:1 (Table 5, columns 1-5). These small changes became incredibly pronounced (at 42.3, 25.4, 25.6, 19.0 and 17.3 times) by recalculating the changes between 0.5 s and  $t \rightarrow \infty$  for each of the lipase addition (at concentrations of 0.01, 0.05, 0.1, 0.5 and 1.0 a.u., Table 5, lines 1-5, respectively), as compared to the very small changes of 0.16 mN/m for the initial mixture (ePC:Chol=9:1). It is interesting that the ST values after 0.5 s for the initial mixture (ePC:Chol=9:1) were a little bit lower (73.44 mN/m) than those for these mixtures with lipase (74.29 mN/m). The only exception found in the case of the extrapolated ST values at maximal time ( $t \rightarrow \infty$ ), which was higher (73.28 mN/m) than those for this mixture with lipase (67.52-71.28 mN/m).

In general, the mean particle diameter (MPD) values decreased drastically by 34.2%, 57.7%, 62.5% and 75.8% by lipase addition from 0.05 to 1.0 a.u., respectively (Table 6). The effective particle diameter (EPD) values changed by 3.7%, -3.6%, 12.6% and

**Table 3: The Current and Equilibrium Surface Tension (ST and eST) Values for the Samples of ePC:Chol=14:1 as Lipid Dispersion (LD14:1) and Lipase (Lip)**

Samples	t=0,5 s	t=1 s	t=3 s	t=5 s	t $\rightarrow\infty$
LD14:1 + 0.01 Lip	73,00	72,93	72,69	72,59	72,32
LD14:1 + 0.05 Lip	72,23	72,11	71,95	71,83	71,72
LD14:1 + 0.1 Lip	73,25	72,56	72,29	72,24	72,06
LD14:1 + 0.5 Lip	72,82	72,75	72,55	72,46	72,21
LD14:1 + 1.0 Lip	72,38	72,24	72,10	72,03	71,74

**Table 4: The Mean Particle Diameter (MPD) and Effective Particle Diameter (EPD) Values for the Samples of ePC:Chol=14:1 in the Presence of Lipase (Lip)**

Samples	MPD, nm	EPD, nm	EPD/MPD
LD14:1 + 0.01 Lip	212.3	395.0	1.80
LD14:1 + 0.05 Lip	146.9	389.5	2.65
LD14:1 + 0.1 Lip	155.3	385.0	2.50
LD14:1 + 0.5 Lip	129.7	379.8	2.93
LD14:1 + 1.0 Lip	138.4	359.2	2.60

**Table 5: The Current and Equilibrium Surface Tension (ST and eST) Values for the Samples of ePC:Chol=9:1 as Lipid Dispersion (LD9:1) and Lipase (Lip)**

Samples	t=0,5 s	t=1 s	t=3 s	t=5 s	t→∞
LD9:1 + 0.01 Lip	74.29	74.10	73.74	73.52	67.52
LD9:1 + 0.05 Lip	74.07	74.06	73.95	73.88	70.00
LD9:1 + 0.1 Lip	74.02	73.96	73.78	73.66	69.92
LD9:1 + 0.5 Lip	74.40	73.96	73.78	73.67	71.36
LD9:1 + 1.0 Lip	74.04	73.62	73.34	73.10	71.28

**Table 6: The Mean Particle Diameter (MPD) and Effective Particle Diameter (EPD) Values for the Samples of ePC:Chol=9:1 in the Presence of Lipase (Lip)**

Samples	MPD, nm	EPD, nm	EPD/MPD
LD9:1 + 0.01 Lip	128.6	295.7	2.30
LD9:1 + 0.05 Lip	84.6	284.8	3.37
LD9:1 + 0.1 Lip	54.4	306.2	5.63
LD9:1 + 0.5 Lip	48.2	258.5	5.36
LD9:1 + 1.0 Lip	31.1	203.8	6.51

31.1% by lipase addition from 0.05 to 1.0 a.u., respectively (Table 6).

#### Lipid Dispersion ePC:Chol=7:3 in the Presence of Lipase

In contrast to previous data (Tables 1, 3 and 5) the small changes of ST values by lipase addition (at maximal concentration of 1.0 a.u.) after 0.5 s, 1 s, 3 s, 5 s and t→∞ found for the mixture of ePC:Chol=7:3 (Table 7, columns 1-4). These small changes became more pronounced (at 1.2, 3.8, 15.0, 1.3 times) by recalculating the changes between 0.5 s and t→∞ for each of the lipase addition (at concentrations of 0.01, 0.05, 0.1 and 0.5 a.u., Table 7, lines 1-4, respectively), as compared to the very small changes of 0.29 mN/m for the initial mixture (ePC:Chol=9:1). It is interesting that the ST values after 0.5 s for the initial mixture (ePC:Chol=7:3) were a little bit lower (73.07 mN/m) than those for these mixtures with lipase (73.29 mN/m).

In general, the mean particle diameter (MPD) values decreased drastically by 29.8%, 38.8% and 62.4% by lipase addition from 0.05 to 0.5 a.u., respectively (Table 8). The effective particle diameter (EPD) values changed by 9.1%, 11.9% and 25.7% by lipase addition from 0.05 to 0.5 a.u., respectively (Table 8).

#### Lipid Dispersion ePC:Chol=1:1 in the Presence of Lipase

The total decrease was about 0.56, 0.54, 0.49, 0.53 and 0.54 mN/m by lipase addition (at maximal concentration of 1.0 a.u.) after 0.5 s, 1 s, 3 s, 5 s and t→∞ for the mixture of ePC:Chol=1:1 as compared to the initial mixture, respectively (Table 9, columns 1-5). The small changes found (at 1.2, 1.3, 1.7, 1.5, 1.2 times) by recalculating the changes between 0.5 s and t→∞ for each of the lipase addition (at concentrations of 0.01, 0.05, 0.1, 0.5 and 1.0 a.u., Table 9, lines 1-5,

**Table 7: The Current and Equilibrium Surface Tension (ST and eST) Values for the Samples of ePC:Chol=7:3 as Lipid Dispersion (LD7:3) and Lipase (Lip)**

Samples	t=0,5 s	t=1 s	t=3 s	t=5 s	t→∞
LD7:3 + 0.01 Lip	73.29	73.26	73.12	73.04	72.94
LD7:3 + 0.05 Lip	73.86	73.32	73.11	72.99	72.75
LD7:3 + 0.1 Lip	73.33	73.31	73.16	73.08	72.99
LD7:3 + 0.5 Lip	73.79	71.20	71.49	73.41	73.40

**Table 8: The Mean Particle Diameter (MPD) and Effective Particle Diameter (EPD) Values for the Samples of ePC:Chol=7:3 in the Presence of Lipase (Lip)**

Samples	MPD, nm	EPD, nm	EPD/MPD
LD7:3 + 0.01 Lip	199.2	294.9	1.48
LD7:3 + 0.05 Lip	139.8	268.2	1.92
LD7:3 + 0.1 Lip	122.0	259.8	2.13
LD7:3 + 0.5 Lip	74.8	219.1	2.93

**Table 9: The Current and Equilibrium Surface Tension (ST and eST) Values for the Samples of ePC:Chol=1:1 as Lipid Dispersion (LD1:1) and Lipase (Lip)**

Samples	t=0,5 s	t=1 s	t=3 s	t=5 s	t→∞
LD1:1 + 0.01 Lip	73.20	73.14	72.90	72.78	72.54
LD1:1 + 0.05 Lip	73.07	73.00	72.71	72.56	72.38
LD1:1 + 0.1 Lip	73.26	72.81	72.62	72.50	72.30
LD1:1 + 0.5 Lip	73.02	72.91	72.66	72.55	72.21
LD1:1 + 1.0 Lip	72.64	72.60	72.41	72.25	72.00

respectively), as compared to the very small changes of 0.55 mN/m for the initial mixture (ePC:Chol=1:1).

In contrast to previous data (Tables 2, 4, 6 and 8), the mean particle diameter (MPD) values increased drastically by 12.5%, 30.5%, -16.6% and 28.2% by lipase addition from 0.05 to 1.0 a.u., respectively (Table 10). The effective particle diameter (EPD) values changed by 6.2%, 7.0%, 5.2% and 8.1% by lipase addition from 0.05 to 1.0 a.u., respectively (Table 10).

## DISCUSSION

The “maximum bubble pressure method” (i.e. BPA-method) is designed to measure surface tension at short surface life times, i.e. for non-equilibrium conditions, which may lead to quantitative differences in the obtained values as compared to the data of well-known works of other authors [36-38] using Langmuir

and other methods [20-22, 36-38] for measuring the equilibrium surface tension. Based on similar considerations particle size measurements were also carried out as quickly as possible (approximately in 10 minutes). It is important to highlight that “the type of diameter obtained with photon correlation spectroscopy is the hydrodynamic diameter, which is the diameter that a sphere would have in order to diffuse at the same rate as the particle being measured” [25]. In the presented systems a relatively broad distribution of particle sizes is present. In this case, the effective particle diameter (EPD) measured is an average diameter calculated in the most simple way, i.e. “by treating the data (the correlation function) without intensity-weighted function” [25]. In contrast, the mean particle diameter (MPD) is an average diameter which is “weighted by the intensity of light scattered by each particle (the translational diffusion coefficient is intensity-weighted)” [25]. More precisely, “the effective

**Table 10: The Mean Particle Diameter (MPD) and Effective Particle Diameter (EPD) Values for the Samples of ePC:Chol=1:1 in the Presence of Lipase (Lip)**

Samples	MPD, nm	EPD, nm	EPD/MPD
LD1:1 + 0.01 Lip	151.5	339.0	2.24
LD1:1 + 0.05 Lip	170.4	317.9	1.87
LD1:1 + 0.1 Lip	197.7	315.2	1.59
LD1:1 + 0.5 Lip	126.3	321.5	2.55
LD1:1 + 1.0 Lip	194.2	311.6	1.60

particle diameter is calculated from the Stokes-Einstein equation (for spheres) from the experimentally determined, translational diffusion coefficient" [25]. That is why the pronounced difference in EPD and MPD values occurred: the EPD to MPD ratios increased from 1.7 to 2.0, from 1.8 to 2.6, from 2.3 to 6.5, from 1.5 to 2.9 for the samples of ePC:Chol at the ratios of 19:1, 14:1, 9:1, 7:1, respectively by lipase concentration increase from 0.05 to 1.0 a.u (Tables 2,4,6,8). The initial EPD/MPD ratio (388.2 to 227.8 nm) of the lipid mixture without lipase was about 1.70.

The specified conditions with large amounts of cholesterol in the system (30-50%) led to a large scatter of data (Tables 8 and 10). We believe that this is due to the non-equilibrium state of the system, especially with the formation of cholesterol domains on particles surface. In this case, an adsorption of lipase occurs mainly at the boundaries of the liquid-expanded layer of ePC and liquid-condensed cholesterol domains on such particle surfaces that is with agreement of the data published recently [36-38]. With lower amounts of cholesterol - 10% (Table 6), the cholesterol domains are not the prevailing structure, and with amounts of cholesterol of 5% or less (Tables 2 and 4), cholesterol molecules are distributed in defects of the liquid-expanded lipid layer [36-38].

Based on the literature data [20-22, 36-38] it can be concluded that the interaction of lipase occurs only with a liquid-expanded lipid layer formed mainly from PC molecules, while there is no interaction with liquid-condensed domains. The MPD and EPD values for the first three systems (Tables 2, 4 and 6) significantly decrease with an increase in the amount of lipase in the system what can be explained by an increase in the degree of organization of ePC molecules in the layer during the lipid-lipase interaction. It is well known that the interaction of lipase with a phospholipid particle at the initial stage occurs to a greater extent due to electrostatic interactions and only in less degree by hydrophobic or Van der Waals interactions [1, 20-22, 36-38]. The priority of electrostatic interactions is associated with the need to overcome the double electric layer of the particle, in order to open the "lid" of the enzyme and then the  $\beta$ -loops that close the hydrophobic region (pocket for triglyceride molecules in the active center of the enzyme) [1, 20-22].

Unlike the monolayers or milk fat droplet systems studied earlier [1, 20-22, 36-38], the systems, studied in this work, lack triglyceride molecules. Therefore, there is no hydrophobic substrate, which in the case of

fat droplets could be the driving force for the further advancement of lipase into the fat particle, i.e. lipase in this case lags behind in the near-surface layer of the particle - at the level of the hydrophilic heads. Lipase, building up in the lipid layer, changes its structure and allows the formation of particles of a smaller diameter in the same way as it happens with the addition of cholesterol to the vesicles of phospholipid [20-22]. With an increase in the amount of lipase in the mixture a large number of ePC-Chol-Lipase particles of a smaller diameter (from 10% to 30% roughly) are obtained. Under equilibrium conditions such a redistribution of particle sizes would take a lot of time but since all the systems in our experiments undergo "ultrasonication" before each measurement the speed of the process increases dramatically.

## CONCLUSIONS

The choice of the "maximum bubble pressure" method was dictated by the need of fast measurements in the lipid-protein systems (even at not equilibrium conditions) what is very important for preserving the native structure of biological systems especially enzymes like lipase. An addition of lipase led to small decrease both, in ST and eST for the samples of ePC:Chol (in the ratios from 19:1 to 1:1). In contrast the mean particle diameter (MPD) and effective particle diameter (EPD) values for the samples of ePC:Chol changed drastically by lipase addition. Probably, the decrease in ST, MPD and EPD occurred by rearrangements of the particles with various size distributions (in such complex colloid dispersions) in the presence of lipase. Thus, the strong interactions of lipase with the mixture of the phospholipid and cholesterol have had completely different features that we expected before the experiments. It seems an interesting a further comparative study of the inorganic and organic compounds with such models of biological membranes for both, fundamental and applied aspects.

## ACKNOWLEDGEMENTS

This work was supported by a grant from the Russian Foundation for Basic Research (project No. 19-03-00717). The authors are thankful to Bondarenko V., Dyakova E. and Rezvantseva Ya. for technical support.

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<https://doi.org/10.3103/S0027131419060130>

Received on 05-11-2020

Accepted on 19-12-2020

Published on 21-12-2020

DOI: <https://doi.org/10.6000/1929-5995.2020.09.08>© 2020 Zaitsev *et al.*; Licensee Lifescience Global.

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